

## Supplementary Material

### Proof for the mathematical derivations for DDMPs with B-Maps

For DDPMs with B-Maps implementation, like the standard DDMP, the optimization is based on maximizing the Evidence Lower Bound (ELBO) [13]:

$$\begin{aligned} \log p(x) \geq & \mathbb{E}_{q(x_1|x_0)}[\log p_\theta(x_0|x_1)] - D_{KL}(q(x_T|x_0)||p(x_T)) \\ & - \sum_{t=2}^T \mathbb{E}_{q(x_t|x_0)}[D_{KL}(q(x_{t-1}|x_t, x_0)||p_\theta(x_{t-1}|x_t))] \end{aligned} \quad (6)$$

In this derivation of the ELBO, the bulk of the optimization cost lies in the summation term. By Bayes rule, we have:  $q(x_{t-1}|x_t, x_0) = \frac{q(x_t|x_{t-1}, x_0)q(x_{t-1}|x_0)}{q(x_t|x_0)}$

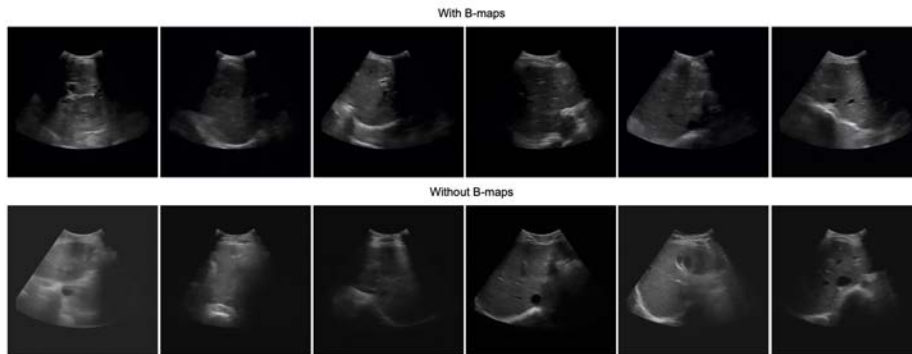
where the first term in the nominator is known Eq. (2) and tractable. Recalling the reparameterization trick, the form of  $q(x_t|x_0)$  and  $q(x_{t-1}|x_0)$  can be recursively derived through repeated applications of the reparameterization trick.

$$\begin{aligned} x_t &= \sqrt{\alpha_t B_t} x_{t-1} + \sqrt{1 - \alpha_t B_t} \epsilon_{t-1}, \quad \text{where } \epsilon_{t-1} \sim \mathcal{N}(0, \mathbf{I}) \\ &= \sqrt{\alpha_t B_t} \sqrt{\alpha_{t-1} B_{t-1}} x_{t-2} + \underbrace{\sqrt{\alpha_t B_t} \sqrt{1 - (\alpha_{t-1} B_{t-1})} \epsilon_{t-2} + \sqrt{1 - (\alpha_t B_t)} \epsilon_{t-1}}_{(1)} \\ &= \sqrt{\alpha_t \alpha_{t-1} B_t B_{t-1}} x_{t-2} + \sqrt{1 - (\alpha_t \alpha_{t-1} B_t B_{t-1})} \epsilon_{t-2} \\ &= \dots \\ &= \sqrt{\prod_{i=1}^t \alpha_i B_i} x_0 + \sqrt{1 - \prod_{i=1}^t \alpha_i B_i} \epsilon, \\ &\sim \mathcal{N}(x_t; \sqrt{\bar{\alpha}_t \bar{B}_t} x_0, (\mathbf{1} - \bar{\alpha}_t \bar{B}_t)) \end{aligned} \quad (7)$$

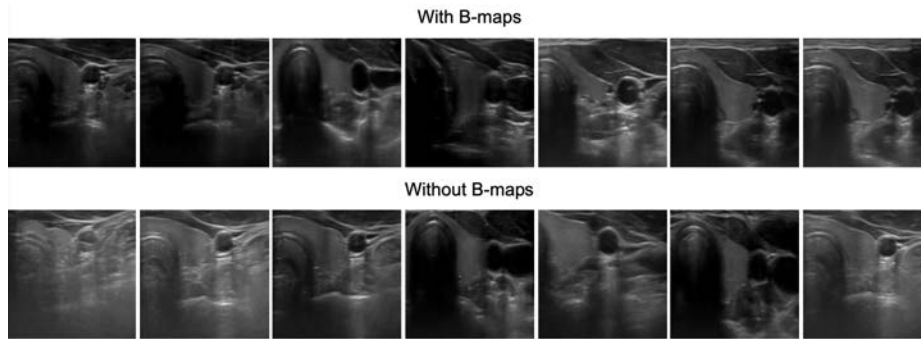
Where, all multiplications are point-wise and in (1) we apply the fact that the sum of two independent Gaussian random variables remains a Gaussian with mean being the sum of the two means, and variance being the sum of the two variances. We have therefore derived like this the Gaussian form of  $q(x_t|x_0)$ , and we can derive  $q(x_{t-1}|x_0)$  the same way. Therefore, knowing the forms of both  $q(x_t|x_0)$  and  $q(x_{t-1}|x_0)$ , we can proceed to calculate the form of  $q(x_{t-1}|x_t, x_0)$ :

$$\begin{aligned} q(x_{t-1}|x_t, x_0) &= \frac{q(x_t|x_{t-1}, x_0)q(x_{t-1}|x_0)}{q(x_t|x_0)} \\ &= \frac{\mathcal{N}(x_t; \sqrt{\alpha_t B_t} x_{t-1}, (\mathbf{1} - \alpha_t B_t) \mathbf{I}) \mathcal{N}(x_{t-1}; \sqrt{\bar{\alpha}_{t-1} \bar{B}_{t-1}} x_0, (\mathbf{1} - \bar{\alpha}_{t-1} \bar{B}_{t-1}) \mathbf{I})}{\mathcal{N}(x_t; \sqrt{\bar{\alpha}_t \bar{B}_t} x_0, (\mathbf{1} - \bar{\alpha}_t \bar{B}_t) \mathbf{I})} \end{aligned} \quad (8)$$

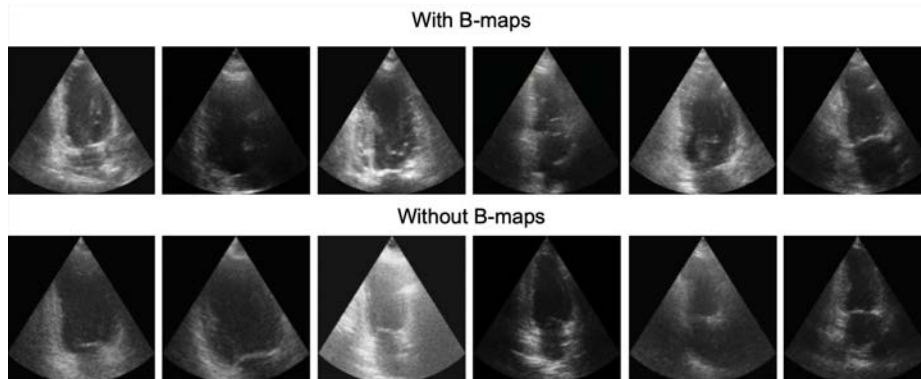
Following the same derivation as in [13] but with our modified Gaussian distributions that depend also on  $B$ , we arrive to the posterior distribution described in the paper.



**Fig. 5. Liver Results:** US images generated with B-Maps (top) exhibit enhanced contrast, especially in the upper regions, compared to those without (bottom).



**Fig. 6. Thyroid Results:** The application of B-Maps in the generation of thyroid US images (top row) results in a clearer delineation and contrast, which is less pronounced in images generated without B-Maps (bottom row).



**Fig. 7. CAMUS Results:** Images generated with B-Maps (top row) have improved contrast in the superior sections, contrasting with the lower contrast seen in the images without B-Maps (bottom row).